Europäisches Patentamt

**European Patent Office**

Office européen des brevets

(11) Publication number: **0 381 694 B1**

(12) **EUROPEAN PATENT SPECIFICATION**

(45) Date of publication of patent specification: **01.06.94**      (51) Int. Cl.⁵: **G01N 21/64**

(21) Application number: **88909172.4**

(22) Date of filing: **16.09.88**

(86) International application number:
**PCT/US88/03193**

(87) International publication number:
**WO 89/03525 (20.04.89 89/09)**

(54) **SINGLE MOLECULE TRACKING.**

(30) Priority: **07.10.87 US 105376**

(43) Date of publication of application:
**16.08.90 Bulletin 90/33**

(45) Publication of the grant of the patent:
**01.06.94 Bulletin 94/22**

(84) Designated Contracting States:
**DE FR GB**

(56) References cited:
**US-A- 4 698 308**

**JOURNAL OF HISTOCHEMISTRY AND CYTOCHEMISTRY, vol. 27, no. 1, 1979, pages 329-334; D.B. KAY et al.: "Imaging in flow"**

**Journal of the Optical Society of America B, Volume 4, no, 2, issued February 1987 (Woodbury, New York), Nguyen et al, "Ultrasensitive Laser - Induced Fluorescence Detection In Hydrodynamically Focused Flows", pages 138-143**

(73) Proprietor: **UNITED STATES DEPARTMENT OF ENERGY**
**1000 Independence Avenue S.W.**
**Washington, D.C. 20585(US)**

(72) Inventor: **SHERA, Edgar, Brooks**
**4 Timber Ridge**
**Los Alamos, NM 87544(US)**

(74) Representative: **Wagner, Karl H. et al**
**WAGNER & GEYER**
**Patentanwälte**
**Gewürzmühlstrasse 5**
**D-80538 München (DE)**

Note: Within nine months from the publication of the mention of the grant of the European patent, any person may give notice to the European Patent Office of opposition to the European patent granted. Notice of opposition shall be filed in a written reasoned statement. It shall not be deemed to have been filed until the opposition fee has been paid (Art. 99(1) European patent convention).

## Description

### BACKGROUND OF THE INVENTION

This invention is generally related to the detection of microscopic particles and, more particularly, to the detection and identification of single molecules. This invention is the result of a contract with the Department of Energy (Contract No. W-7405-ENG-36).

The capability for detecting microscopic particles has been proceeding toward smaller particles. For many applications it is essential that microscopic particles be detected in a liquid-phase environment. Existing techniques, usable in a liquid-phase environment, are based on optical trapping and on flow separation using hydrodynamically focused flows. Molecular identification by laser-induced fluorescence has been used with hydrodynamically focused flows to permit the detection of large and highly fluorescent molecules using conventional photomultiplier tubes to detect the molecule fluorescence.

Optical trapping and manipulation of viruses and bacteria are taught in A. Ashkin et al., "Optical Trapping and Manipulation of Viruses and Bacteria." Science 235, 1517 (1987). Rayleigh- and Mie-sized particles, i.e., a particle size range from about 10 μm down to a few angstroms, have been trapped using optical forces to confine the particles. The only method of identification taught by Ashkin et al. appears to be a size determination from a scattering comparison with a sphere of known size. Further, a large number of particles are trapped.

A hydrodynamically focused flow system is taught by D. C. Nguyen et al., "Ultrasensitive Laser-Induced Fluorescence Detection in Hydrodynamically Focused Flows," J. Opt. Soc. Am. B4, 138 (1987), and D. C. Nguyen et al., "Detection of Single Molecules of Phycoerythrin in Hydrodynamically Focused Flows by Laser Induced Fluorescence," Anal. Chem. 59, 2158 (1987). As taught therein, improvements in the optics and reductions in the size of the probe volume provide a sensitivity effective to detect a single species containing the fluorescence equivalent of eight rhodamine-6G chromophores. The detection of single molecules of the highly fluorescent species phycoerythrin is reported.

A variety of modifications are reported to enhance the detection sensitivity of the device, with the improvements being related to conventional optics and flow dynamics, and with a sample volume reduction from 11 pL to 0.6 pL producing a concomitant reduction in detected background radiation. The reported sensitivities do not, however, enable the device to detect individual molecules that might typically be of interest, such as fluorophore-tagged versions of the base molecules that make up the DNA polymer.

Thus, available methods and apparatus for detecting particles in a flow stream do not provide the sensitivity for detecting individual molecules that might typically be encountered in immunofluorescence assay, flow cytometry, liquid chromatography, and similar applications. An agglomeration of molecules might be detected, but single molecules could not then be identified. This lack of capabilities in the art is overcome by the present invention and improved method and apparatus are provided for detecting a single modestly fluorescent molecule.

Accordingly, it is an object of the present invention to reliably detect a single fluorescent molecule.

Another object is to reliably detect single fluorescent molecules with a fluorescence equivalent to fluorescently-labeled versions of the bases forming the DNA polymer.

Yet another object is to provide an increased capability of rejecting background radiation.

One other object is to minimize the resolution limitations inherent in conventional optics while maintaining a large field of view.

### SUMMARY OF THE INVENTION

To achieve the foregoing and other objects, and in accordance with the purposes of the present invention, as embodied and broadly described herein, the apparatus of this invention may comprise a molecule detection system for identifying individual molecular characteristic emissions in a train of molecules in a flow cell. A position sensitive sensor means is located effective to detect emissions from molecules within the flow cell and to assign spatial and temporal coordinates for the detected emissions. A computer predicts spatial and temporal coordinates for a molecule in the laminar flow as a function of the detected coordinates of said detected emissions. Comparison means then compare subsequently detected spatial and temporal coordinates with the predicted spatial and temporal coordinates to determine whether said subsequently detected emissions originated from an excited molecule in the train of molecules. Thus, molecular emissions can be distinguished from background emissions and identified with a particular molecule in the sequence.

In another characterization of the present invention, a detection method is provided for identifying individual molecules within a flow cell from characteristic molecular emissions. Molecular emissions from within the flow cell are detected with a position sensitive sensor. Spatial and temporal co-

ordinates are then assigned to the detected emissions. Based on known flow characteristics in the flow cell, spatial and temporal coordinates are predicted for a molecule in the flow as a function of a first detected emission within the flow cell. The detected spatial and temporal coordinates of subsequent emissions are compared with predicted spatial and temporal coordinates to determine whether a detected emission originated from a molecule in the train of molecules. Thus, molecular emissions are distinguished from background events and a single molecule can be identified during passage through the flow cell.

BRIEF DESCRIPTION OF THE DRAWINGS

The accompanying drawings, which are incorporated in and form a part of the specification, illustrate an embodiment of the present invention and, together with the description, serve to explain the principles of the invention. In the drawings:
    FIGURE 1 is a block diagram schematic of the present invention.
    FIGURE 2 is a detail of the system flow cell in pictorial form.
    FIGURE 3 is flow chart for distinguishing and evaluating individual molecules in the flow cell.

DETAILED DESCRIPTION OF THE INVENTION

Referring now to Figure 1, there is shown in block diagram schematic form a molecule detection system according to the present invention. The laser excitation system is generally well known and described in the Nguyen et al. articles, hereinabove referenced. Laser 10 is selected with a wavelength effective to fluoresce a selected fluorophore for identifying the molecule to be detected. The output from laser 10 is conventionally passed through half-wave plate 12 and polarizing prism 14, wherein the output power of laser 10 can be adjusted by varying the angle of plate 12 with respect to prism 14. The laser output power and the polarization can be adjusted to minimize background counts.

Mirror 16 directs the laser beam through lens 18 to focus within flow cell 22 for activating fluorophores attached to molecules in the sample stream. As shown in Figure 2, sample stream 42 is orthogonal to focused laser beam 46. Sample stream 42 passes within a surrounding hydraulic sheath 44 to provide hydrodynamic focusing of the flow within flow cell 22.

Referring again to Figure 1, the output from flow cell 22 is optical signal 20 with information on the fluorescing molecules within flow cell 22. Optical signal 20 is focused by microscopic objective lens 24 and filtered by spectral filter 25 to remove wavelengths which are not of interest. The output

optical signal is provided to a position-sensitive sensor 26. In one embodiment, position-sensitive detector 26 is formed from a microchannel plate position-sensitive detector (MCP) and operation is hereinafter discussed with respect to a MCP.

A position-sensitive detector or MCP 26 outputs a signal which is indicative of the occurrence of a photon event within flow cell 22 and also location data functionally related to the spatial coordinates of the photon event. Spatial coordinates are provided to digitizer 28 and combined with a temporal input from timer 32 to provide at least a three-dimensional (x, y, t) location for the photon event. Photon event coordinates are output from digitizer 28 to memory 34 for subsequent processing by computer station 36.

Referring now to position-sensitive sensor 26, it is desirable to have the resolution of the system, and related position accuracy, limited by the system optics rather than a MCP. Conventional MCPs may have a positional resolution of 500-1000 pixels in each dimension. If two pixels cover each Rayleigh limit, resolution is limited by the optics and a field of view of 100-200 microns in diameter is provided by objective lens 24. By way of example, the Rayleigh limit at a wavelength of 560 nm is about 0.4 microns. Thus, a position accuracy of 1 micron requires only a precision of ± 2 pixels. A suitable MCP is available as model P4146M from ITT. Electro-Optical Products Division.

Digitizer 28 provides spatial and temporal coordinate data in a format that is suitable for direct storage in memory 34 and can operate in real time. Conventional MCP position circuitry digitizes in about 5 $\mu$s. This digitizing interval can be reduced to about 1 $\mu$s, or less, with custom circuitry, if a high data rate operation is desirable. A 1 $\mu$s digitizing interval would enable a maximum photon detection rate of 1 MHz; or, e.g., 170 photons during the transit time predicted by Nguyen et al. for a system comparable to flow cell 22. As discussed below, the detection of only a few photons can provide for reliable molecule identification even with a relatively unsophisticated data reduction algorithm. The flow velocity and laser intensity can readily be adjusted to provide a data rate and observation time suitable for particular applications.

It will be appreciated that the above system provides the position accuracy needed to identify a photon event within 1 micron or less. With a suitable width of the laser beam in the longitudinal direction as, for example, by evanescent wave illumination, this accuracy thus produces an effective sample volume of $10^{-18}$ m$^3$, or $10^{-3}$ pL, a sample volume reduction by about 500 over the 0.6 pL value discussed in Nguyen et al. The effective sample volume allows the system to discriminate against photon events which do not originate with a

fluorescing molecule since only a few scattering events will randomly occur within the effective sample volume. The laminar flow provides known trajectories for molecules having a known velocity. Detected photon events can be compared with predicted molecule coordinates and photon events which do not correspond with predicted coordinates can be disregarded. This capability effectively provides a moving sample volume as small as $10^{-3}$ pL within which the presence of a molecule can be reliably predicted.

The above system has been described above using a hydrodynamic flow regime and a fluorescing molecule. However, the functional principles apply equally to any dynamic system which can maintain a predictable flow of molecules or small particles in sequence through a detector. Likewise, laser-induced fluorescence is a convenient technique to tag and identify molecules. All that is needed, however, is a detectable emission from the molecule or particle. Alternatively, other molecular emissions, such as electrons, gamma rays, and the like, can be detected by suitable position-sensitive devices. The present invention broadly contemplates hydrodynamic and aerodynamic flow regimes, as well as molecular emissions of all kinds.

Referring now to Figure 3, there is shown a flow diagram for exemplary software for determining the presence of a molecule in an effective sample volume. On the occurrence of a photon event 48 from MCP 26 (Figure 1), the event coordinates $(x_e, y_e, t_e)$ are input 52 and a bin is defined 54 with coordinates $(x_e, y_e, t_n)$ where $t_n$ is normalized 53 to the time a molecule having the spatial coordinates would have entered the field of view defined by objective lens 24 (Figure 1). The new defined bin is compared 56 with existing bins. If the new bin does not exist, the new bin is stored 58 to represent an initial event and the contents of bin file 58 are updated 62.

If existing bin coordinates accommodate the defined event bin coordinates 54, the event is assigned to that particular bin 64. Bins continue to accumulate 64 events until the bin temporal coordinate indicate that the bin has passed outside the field of view of the system.

Timer 66 periodically causes the bins to be examined 68 to determine whether a bin is still within the field of view or whether a molecule was present in that bin. Bins that accumulate a large number of events have a higher probability of containing an actual molecule than bins with fewer events. The small effective sample volume which is provided according to the present invention can produce a clear separation between bins that contain molecules and those that contain only random background events. After the bin count is processed, the bin is cleared 74 for reuse. If the

presence of a molecule is indicated, the fluorescence data can be processed 72 for the particular determination being made by the system. More complex data reduction algorithms might further consider diffusion and other departures from laminar flow that can occur in various applications.

The capability to track and identify an individual molecule provides applications which are not possible using conventional photomultiplier tubes. In one important application, the system might be adapted to detect and identify individual bases forming a DNA sequence. A plurality of laser wavelengths, alone or in combination with separate filters 25 and detectors 26 (Figure 1), could be used to excite individual molecules as they pass through the sample flow cell 22 to identify fluorescent base-specific labels which are attached to the molecules. The track of a molecule will alternately appear or disappear to enable molecule identification during the excitation sequence. Several molecules may be simultaneously present in flow cell 22 and be individually tracked for identification.

While a single MCP system has been discussed above, it may be desirable to provide two orthogonally placed MCPs to increase the number of photons which are collected during transit of the molecule through flow cell 22 and to provide additional spatial information. Detected photon events would be correlated to provide complete three-dimensional spatial coordinates. A detected photon in each of two orthogonally placed detectors will, in principle, enable a trajectory to be predicted, such that the presence of a third photon on the computed four-dimensional trajectory is evidence of a molecule passage.

It will be appreciated that the detection of these few photons in the available transit times produces an infinitesimal probability of missing a molecule entirely. By way of example, in a 2 MCP geometry, and a 170 µs transit time, shown by Nguyen et al., supra, in Table 3, it can be estimated that each detector will accumulate 8 real and 40 background photons. Thus, the 2 MCPs will detect a mean number of 16 photons, providing a probability of less than $10^{-4}$ of detecting fewer than the 4 photons needed for molecule detection.

The software discussed for Figure 3 can be provided for each MCP and the bins merged during the processing. A merger determination could be made on the basis of the available common information, i.e., time coordinates. Bins might be examined for merging only after a minimum number of events are accumulated in that bin, thereby assuring that the time coordinates of both bins are sufficiently well-determined to make a valid comparison for the merger. The bin with the large number of accumulated events might be selected for the merged bin, whereby all subsequent photon

events on the bin trajectory are assigned to a single bin.

The foregoing description of the preferred embodiment of the invention has been presented for purposes of illustration and description. It is not intended to be exhaustive or to limit the invention to the precise form disclosed, and obviously many modifications and variations are possible in light of the above teaching. The embodiment was chosen and described in order to best explain the principles of the invention and its practical application to thereby enable others skilled in the art to best utilize the invention in various embodiments and with various modifications as are suited to the particular use contemplated. It is intended that the scope of the invention be defined by the claims appended hereto.

**Claims**

1. A molecule detection system, comprising:
   a flow cell for passing a train of molecules in laminar flow;
   laser means for exciting said molecules to emit photons at a selected wavelength;
   position sensitive sensor means effective to detect said photon emissions within said flow cell and assign spatial and temporal coordinates for said detected photons;
   computer means for predicting spatial and temporal coordinates for a molecule in said laminar flow as a function of said detected photon; and
   comparison means for comparing subsequent detected spatial and temporal coordinates with said predicted spatial and temporal coordinates to determine whether a subsequently detected photon originated from an excited molecule in said train of molecules.

2. A detection system according to Claim 1, wherein said position sensitive sensor means includes at least one microchannel plate sensor for outputting said spatial coordinates.

3. A detection system according to claim 1, wherein said position sensitive sensor means has a position accuracy effective for said computer means to create from said predicted coordinates a moving sample volume effective to functionally eliminate background signals from consideration.

4. A detection system for identifying individual molecules having characteristic emissions in a flow train of molecules in a flow cell, comprising:
   position sensitive sensor means effective to detect emissions from said molecules within said flow cell and assign spatial and temporal coordinates for said detected emissions;
   computer means for predicting spatial and temporal coordinates for a molecule in said flow train as a function of said detected emissions; and
   comparison means for comparing subsequent detected spatial and temporal coordinates with said predicted spatial and temporal coordinates to determine whether said subsequently detected emissions originate from an excited molecule in said train of molecules.

5. A detection system according to claim 4, wherein said position sensitive sensor means includes at least one microchannel plate sensor for outputting said spatial coordinates.

6. A detection system according to claim 4, wherein said position sensitive sensor means has a position accuracy effective for said computer means to create from said predicted coordinates a moving sample volume effective to functionally eliminate background signals from consideration.

7. A detection method for identifying individual molecules having a characteristic emission in a flow train, comprising:
   detecting in position sensitive sensor means molecular emissions within said flow train;
   assigning spatial and temporal coordinates for said detected emissions;
   predicting spatial and temporal coordinates for a molecule as a function of said first detected emissions; and
   comparing subsequent detected spatial and temporal coordinates with said predicted spatial and temporal coordinates to determine whether said subsequently detected emissions originate from a molecule in said train of molecules.

8. A method according to Claim 7, wherein detecting emissions includes the step of focusing products from said emissions on at least one microchannel plate sensor.

9. A method according to Claim 7, wherein said predicting spacial and temporal coordinates further defines a moving sample window for molecule detection effective to discriminate background emission events from molecule emission events.

**10.** A method according to Claim 7, wherein said emission products are photons.

**11.** A method according to Claim 10, further including the step of irradiating said molecules with a laser to induce a fluorescence for emitting said photons.

**12.** A method according to Claim 7, further including the step of hydrodynamically focusing said flow train within a flow cell.

**Patentansprüche**

1. Moleküldetektiersystem, das folgendes aufweist: eine Strömungszelle zum Hindurchlassen einer Folge oder Reihe von Molekülen in einer Laminarströmung;
Lasermittel zum Erregen der Moleküle zum Abgeben oder Emittieren von Photonen mit einer ausgewählten Wellenlänge;
positionsempfindliche Sensormittel, die wirksam sind zum Detektieren der Photonenemissionen innerhalb der Strömungszelle und den detektieren Photonen räumliche und zeitliche Koordinaten zuordnen;
Computermittel zum Vorhersagen räumlicher und zeitlicher Koordinaten für ein Molekül in der Laminarströmung als eine Funktion des detektierten Photons; und
Vergleichsmittel zum Vergleichen nachfolgender detektierter, räumlicher und zeitlicher Koordinaten mit den vorhergesagten räumlichen und zeitlichen Koordinaten zum Feststellen, ob ein nachfolgend detektiertes Photon von einem erregten Molekül in der Folge oder Reihe von Molekülen stammt.

2. Detektiersystem gemäß Anspruch 1, wobei die positionsempfindlichen Sensormittel mindestens einen Mikrokanalplattensensor zum Abgeben der räumlichen Koordinaten umfassen.

3. Detektiersystem nach Anspruch 1, wobei die positionsempfindlichen Sensormittel eine Positionsgenauigkeit besitzen, die wirksam ist für die Computermittel um aus den vorhergesagten Koordinaten ein sich bewegendes Probenvolumen zu erzeugen, was in effektiver Weise funktionell die Hintergrundsignale aus der Betrachtung eliminiert.

4. Detektiersystem zum Identifizieren individueller Moleküle mit charakteristischen Emissionen in einer Strömungsreihe oder Folge von Molekülen in einer Strömungszelle, das folgendes aufweist:
positionsempfindliche Sensormittel, die das

Detektieren von Emissionen von den Molekülen innerhalb der Strömungszelle bewirken und räumliche und zeitliche Koordinaten für die detektierten Emissionen zuordnen;
Computermittel zum Vorhersagen räumlicher und zeitlicher Koordinaten für ein Molekül in der Strömungsreihe oder Folge als eine Funktion der detektierten Emissionen; und
Vergleichsmittel zum Vergleichen nachfolgender detektierter, räumlicher und zeitlicher Koordinaten mit den vorhergesagten räumlichen und zeitlichen Koordinaten um festzustellen, ob die nachfolgend detektierten Emissionen von einem erregten Molekül in der Folge oder Reihe von Molekülen stammen.

5. Detektiersystem nach Anspruch 4, wobei die positionsempfindlichen Sensormittel mindestens einen Mikrokanalplattensensor umfassen zum Abgeben der räumlichen Koordinaten.

6. Detektiersystem nach Anspruch 4, wobei die positionsempfindlichen Sensormittel eine Positionsgenauigkeit besitzen, die wirksam ist für die Computermittel um aus den vorhergesagten Koordinaten ein sich bewegendes Probenvolumen zu erzeugen, was in effektiver Weise funktionell die Hintergrundsignale aus der Betrachtung eliminiert.

7. Detektierverfahren zum Indentifizieren individueller Moleküle mit einer charakteristischen Emission in einer Strömungsreihe oder Folge, das folgendes aufweist:
Detektieren von molekularen Emissionen innerhalb der Strömungsreihe und zwar in positionsempfindlichen Sensormitteln;
Zuordnen räumlicher und zeitlicher Koordinaten für die detektierten Emissionen;
Vorhersagen räumlicher und zeitlicher Koordinaten für ein Molekül als eine Funktion der ersten detektierten Emissionen; und
Vergleichen nachfolgender detektierter, räumlicher und zeitlicher Koordinaten mit den vorhergesagten räumlichen und zeitlichen Koordinaten um festzustellen, ob die nachfolgend detektierten Emissionen von einem Molekül in der Folge oder Reihe von Molekülen stammen.

8. Verfahren nach Anspruch 7, wobei das Detektieren von Emissionen den Schritt des Fokusierens von Produkten der Emissionen auf mindestens einem Mikrokanalplattensensor umfaßt.

9. Verfahren nach Anspruch 7, wobei das Vorhersagen räumlicher und zeitlicher Koordinaten ferner das Definieren eines sich bewegenden Probenfensters für die Moleküldetektierung de-

finiert zum effektiven Unterscheiden von Hintergrundemissionsereignissen von Molekülemissionsereignissen.

**10.** Verfahren nach Anspruch 7, wobei die Emissionsprodukte Photonen sind.

**11.** Verfahren nach Anspruch 10, das ferner den Schritt des Bestrahlens der Moleküle mit einem Laser umfaßt zum Induzieren einer Fluoreszenz zum Emittieren der Photonen.

**12.** Verfahren nach Anspruch 7, das ferner den Schritt des hydrodynamischen Fokusierens der Strömungsreihe oder Folge innerhalb einer Strömungszelle umfaßt.

**Revendications**

**1.** Système de détection de molécules, comprenant :
- une cellule à écoulement pour faire passer un train de molécules dans un écoulement laminaire;
- des moyens à laser pour exciter lesdites molécules pour émettre des photons à une longueur d'onde choisie;
- des moyens de détection sensibles à la position, efficaces pour détecter lesdites émissions de photons dans ladite cellule à écoulement et pour attribuer des coordonnées spatiales et temporelles pour lesdits photons détectés;
- des moyens de calcul pour prédire les coordonnées spatiales et temporelles pour une molécule dans ledit écoulement laminaire en fonction desdits photons détectés; et
- des moyens de comparaison pour comparer des coordonnées spatiales et temporelles détectées ultérieures et lesdites coordonnées spatiales et temporelles prédites, pour déterminer si un photon détecté ultérieurement provenait d'une molécule excitée dans ledit train de molécules.

**2.** Système de détection selon la revendication 1, dans lequel lesdits moyens de détection sensibles à la position incluent au moins un détecteur à galette de microcanaux pour fournir en sortie lesdites coordonnées spatiales.

**3.** Système de détection selon la revendication 1, dans lequel lesdits moyens de détection sensibles à la position ont une précision de position efficace pour que lesdits moyens de calcul créent, à partir desdites coordonnées prédites,

un volume d'échantillon mobile efficace pour que, d'une manière fonctionnelle, des signaux de fond ne soient pas pris en considération.

**4.** Système de détection pour identifier des molécules individuelles qui ont des émissions caractéristiques dans un train d'écoulement de molécules dans une cellule d'écoulement, comprenant :
- des moyens de détection sensibles à la position, efficaces pour détecter des émissions provenant desdites molécules dans ladite cellule à écoulement et pour attribuer des coordonnées spatiales et temporelles pour lesdites émissions détectées;
- des moyens de calcul pour prédire les coordonnées spatiales et temporelles pour une molécule dans ledit train d'écoulement en fonction desdites émissions détectées; et
- des moyens de comparaison pour comparer des coordonnées spatiales et temporelles détectées ultérieures et lesdites coordonnées spatiales et temporelles prédites, pour déterminer si lesdites émissions détectées ultérieurement proviennent d'une molécule excitée dans ledit train de molécules.

**5.** Système de détection selon la revendication 4, dans lequel lesdits moyens de détection sensibles à la position incluent au moins un détecteur à galette de microcanaux pour fournir en sortie lesdites coordonnées spatiales.

**6.** Système de détection selon la revendication 4, dans lequel lesdits moyens de détection sensibles à la position ont une précision de position efficace pour que lesdits moyens de calcul créent, à partir desdites coordonnées prédites, un volume d'échantillon mobile efficace pour que, d'une manière fonctionnelle, des signaux de fond ne soient pas pris en considération.

**7.** Procédé de détection pour identifier des molécules individuelles qui ont une émission caractéristique dans un train d'écoulement, comprenant :
- la détection, dans des moyens de détection sensibles à la position, d'émissions moléculaires dans ledit train d'écoulement;
- l'attribution de coordonnées spatiales et temporelles pour lesdites émissions détectées;
- la prédiction de coordonnées spatiales et temporelles pour une molécule en fonc-

tion desdites premières émissions détectées; et

- la comparaison de coordonnées spatiales et temporelles détectées ultérieures et desdites coordonnées spatiales et temporelles prédites, pour déterminer si lesdites émissions détectées ultérieurement proviennent d'une molécule dans ledit train de molécules.

8. Procédé selon la revendication 7, dans lequel la détection d'émissions inclut l'étape de focalisation de produits provenant desdites émissions sur au moins un détecteur à galette de microcanaux

9. Procédé selon la revendication 7, dans lequel lesdites coordonnées spatiales et temporelles prédites définissent en outre une fenêtre d'échantillon mobile pour la détection de molécules, efficace pour discriminer les événements d'émission de fond des événements d'émission de molécules.

10. Procédé selon la revendication 7, dans lequel lesdits produits d'émission sont des photons.

11. Procédé selon la revendication 10, incluant en outre l'étape d'irradiation desdites molécules avec un laser, pour induire une fluorescence pour l'émission desdits photons.

12. Procédé selon la revendication 7, incluant en outre l'étape de focalisation hydrodynamique dudit train d'écoulement dans une cellule à écoulement.
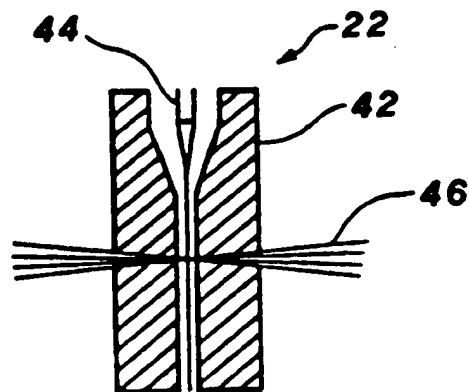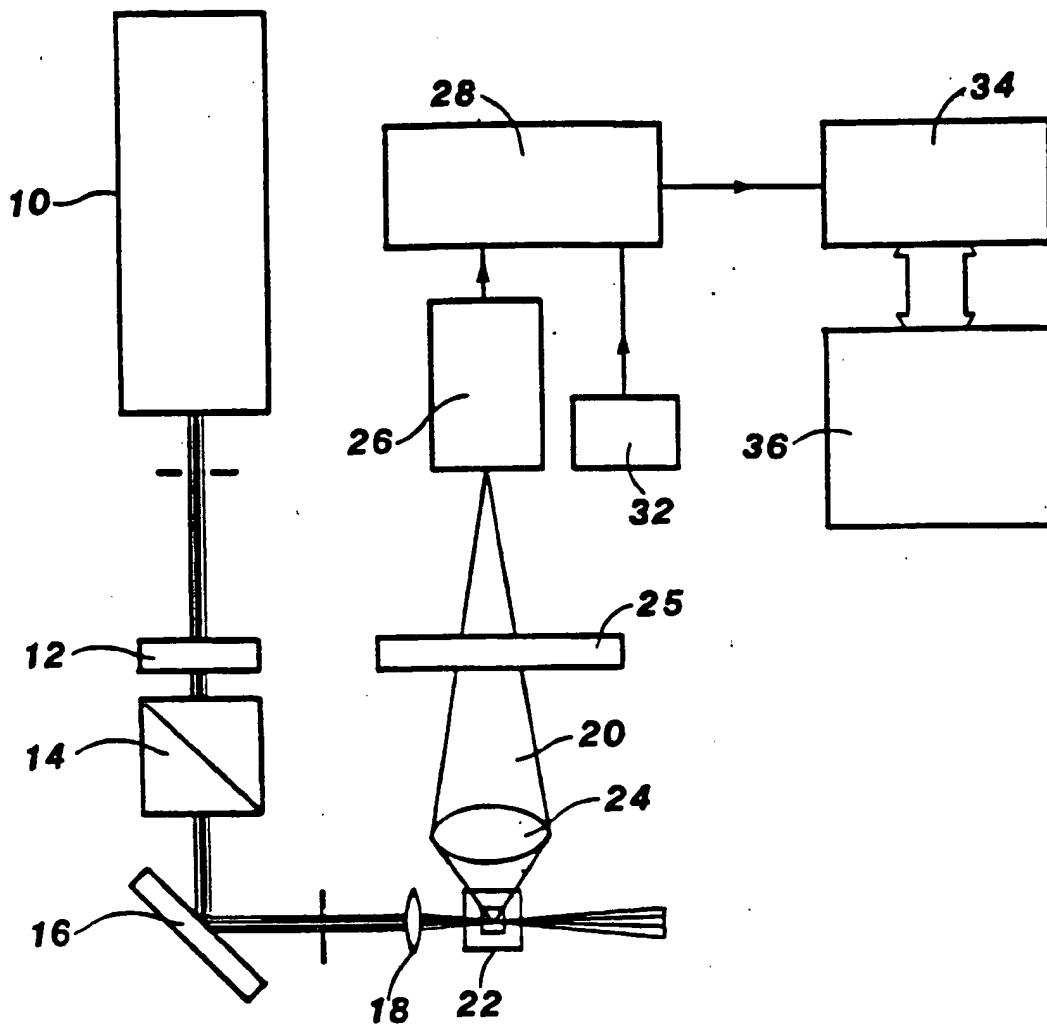
# Fig 1



# Fig. 2

# *Fig. 3*

Photon Event
Signal *48*

COORDINATES
xe, ye, te — *52*

COMPUTE
ENTRANCE
TIME, tn — *53*

DEFINE BIN
xe, ye, te — *54*

STORE BIN
COORDINATES — *58*

EXISTING
BIN ? — *56*

N

Y

UPDATE BIN
FILE — *62*

INCREASE
BIN COUNT — *64*

TIME OUT ? — *66*

BIN CONTAIN
MOLECULE ? — *68*

N

CLEAR
BIN — *74*

Y

PROCESS
FLUORESCENCE
DATA — *72*

MOLECULE
IDENTITY